

Partial Skeletal Muscle Grafts for Prosthetic Control

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Abstract

Background: Nonvascularized partial skeletal muscle grafts are notorious for their limited force-generating capacity and tendency to degenerate in the absence of reinnervation [1-3]. Accompanied by peripheral nerve implantation, however, partial muscle grafts can survive and transmit detectable electromyographic (EMG) signals capable of prosthetic control [4]. Our study investigated partial muscle graft survival in the construction of regenerative peripheral nerve interfaces (RPNI) and further characterized their electrophysiological properties across various muscle donor sites.

Methods: Twenty F344 rats were assigned to 1 of 5 groups based on muscle graft type used for RPNI construction: 1) control-whole extensor digitorum longus; 2) partial biceps femoris; 3) partial rectus femoris; 4) partial lateral gastrocnemius; and 5) partial vastus medialis. Each graft of approximately 140-mg was transferred to the femur, wrapped in small intestinal submucosa for tissue isolation, and implanted with the transected common peroneal nerve. After 4 months of RPNI recovery, *in situ* EMG (Figure 1) and force testing were performed.

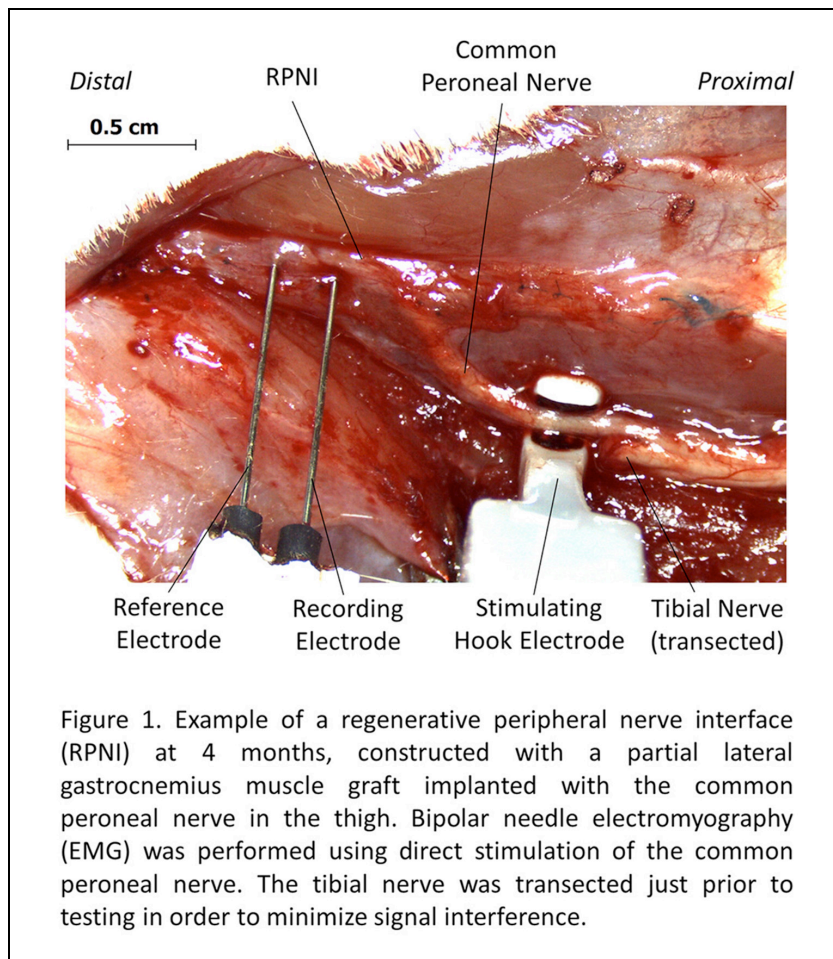


Figure 1. Example of a regenerative peripheral nerve interface (RPNI) at 4 months, constructed with a partial lateral gastrocnemius muscle graft implanted with the common peroneal nerve in the thigh. Bipolar needle electromyography (EMG) was performed using direct stimulation of the common peroneal nerve. The tibial nerve was transected just prior to testing in order to minimize signal interference.

Results: Twelve of 16 partial muscle RPNI demonstrated detectable EMG function at 4 months. Significant differences between control RPNI (n=4) and functional partial muscle RPNI (n=12) included average mass (118 ± 42 mg vs. 66 ± 25 mg), EMG peak-to-peak amplitude (6.7 ± 2.3 mV vs. 1.5 ± 1.6 mV), and maximum tetanic force (729 ± 666 mN vs. 175 ± 154 mN). Outcomes by group for all RPNI (n=20) are depicted in Figure 2. RPNI mass was the overriding significant predictor of EMG peak-to-peak amplitude ($p < 0.001$). After adjusting for RPNI mass, donor muscle type showed no correlation with partial muscle EMG signal strength.

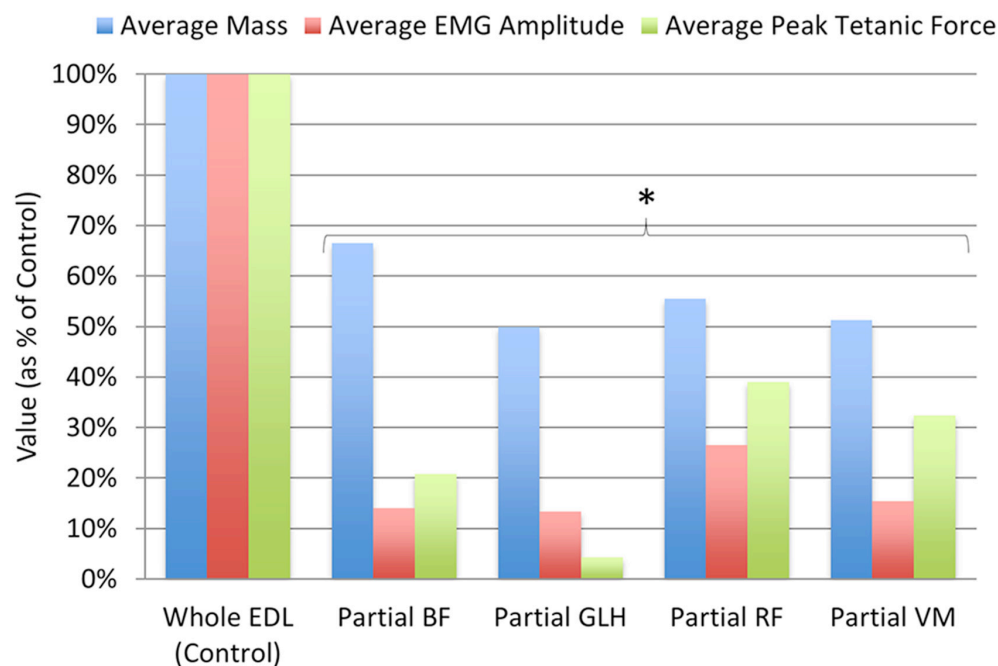


Figure 2. Comparison of control versus partial muscle RPN mass, EMG peak-to-peak amplitude, and peak tetanic force at 4 months. Values for partial muscle RPN groups are expressed as percentages of control group values, with $n=4$ per group. All values for partial muscle RPN groups were significantly lower than their control group counterparts (*, $p < 0.05$). *EDL*, extensor digitorum longus; *BF*, biceps femoris; *GLH*, gastrocnemius, lateral head; *RF*, rectus femoris; *VM*, vastus medialis.

Conclusions: Partial muscle graft RPNs transmit detectable EMG signals with a 75% success rate at 4 months. This proof of concept feasibility underscores the potential to develop and refine partial muscle graft-based interfaces to harness peripheral nerve signals for high-fidelity prosthetic control in amputees. While signal size remains favorable (i.e. 10-50 times larger than signals recorded directly from peripheral nerves) [5], further studies are warranted for optimization of partial muscle graft regeneration and methods of signal acquisition.

References

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